

Wave shape function

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Outline

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- Instantaneous Frequency and Wave-Shape Function (WSF)
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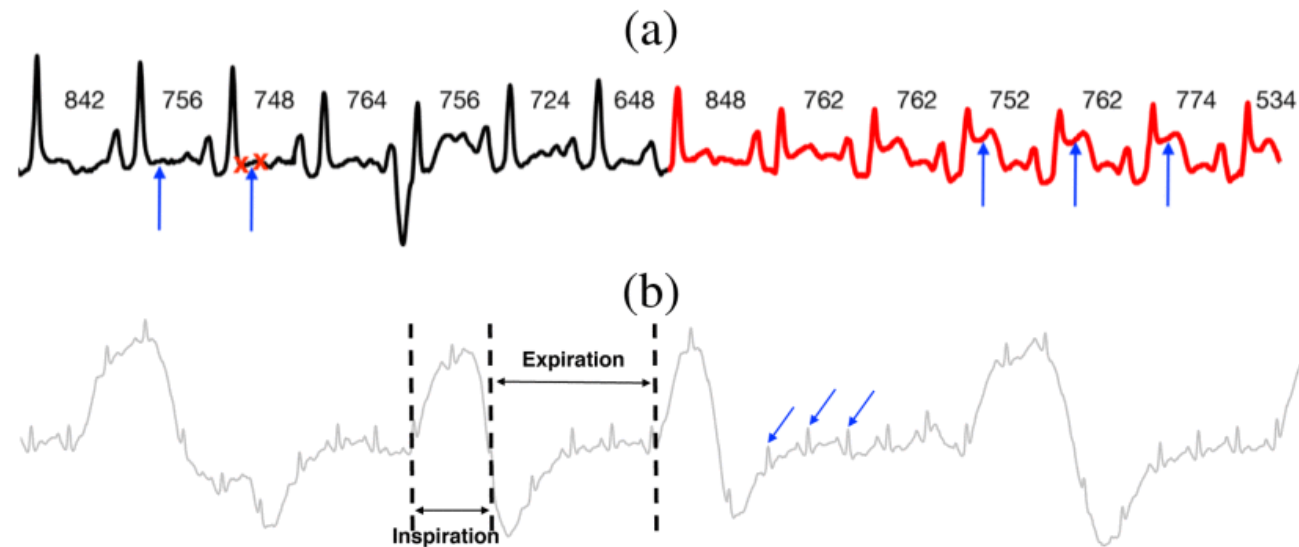
Introduction

Multi-component oscillating signals

- Time-varying frequencies
- Time-varying amplitudes
- Non-sinusoidal oscillation modes

Fields

- Biomedicine
- Mechanical systems
- Music signal



An illustration of two complicated non-sinusoidal oscillatory signals [1].

[1] M. A. Colominas and H. -T. Wu, "Decomposing Non-Stationary Signals With Time-Varying Wave-Shape Functions," in IEEE Transactions on Signal Processing, vol. 69, pp. 5094-5104, 2021

Adaptive Harmonic Model

For an simplest adaptive harmonic model [2]:

$$f(t) = \sum_{k=1}^K A_k(t) \cos(2\pi\phi_k(t))$$

with $A_k(t), \phi'_k(t) > 0 \forall t$.

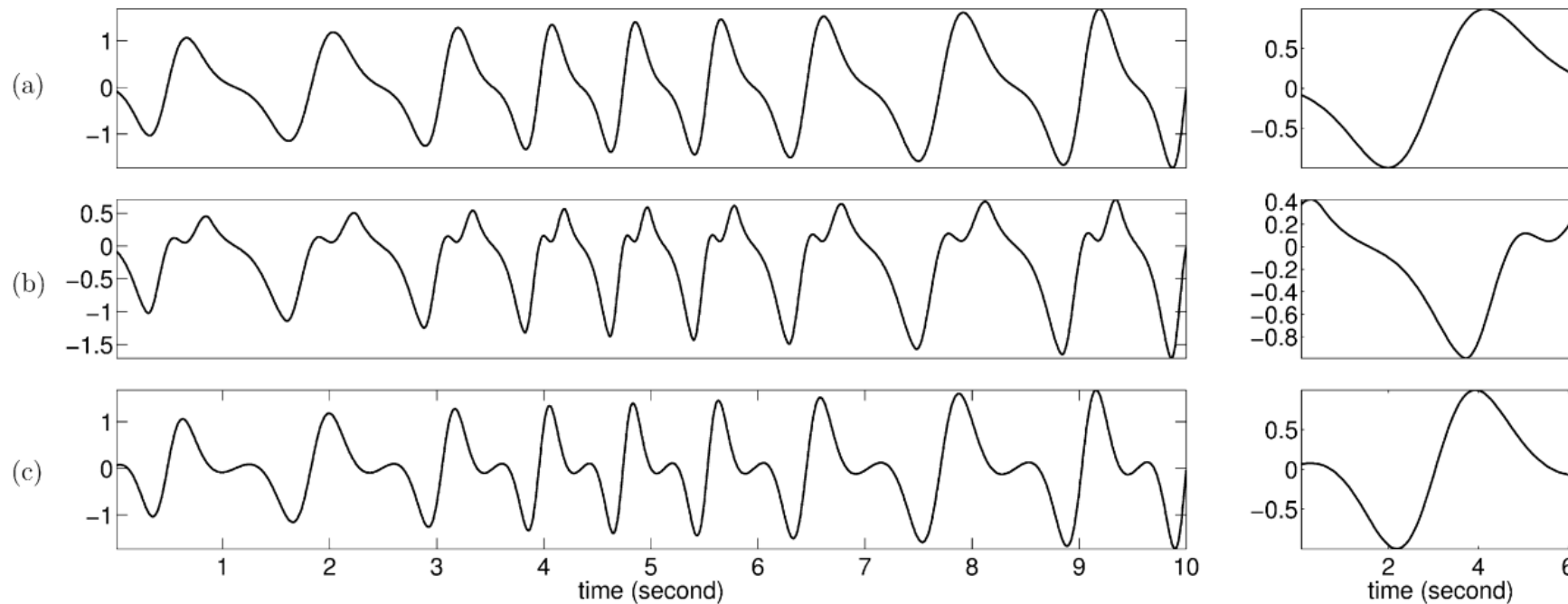
- $A_k(t)$: amplitude modulation (slowly change) $A_k(t) > 0, |A'_k(t)| \leq \epsilon\phi'_k(t)$
- $\phi_k(t)$: phase function (monotonic increasing) $\phi'_k(t) > 0$
- $\phi'_k(t)$: instantaneous frequency (slowly change) $|\phi''_k(t)| \leq \epsilon\phi'_k(t)$
- $A_k(t) \cos(2\pi\phi_k(t))$: intrinsic mode type function

Wave-shape function (WSF)

The model for more real-life situation [3]:

$$f_{fix}(t) = A(t)s(2\pi\phi(t))$$

where $s(t)$ is a real 1-periodic function with the unitary L^2 norm, that is for all t . The periodic signal $s(t)$ is called the wave-shape function.



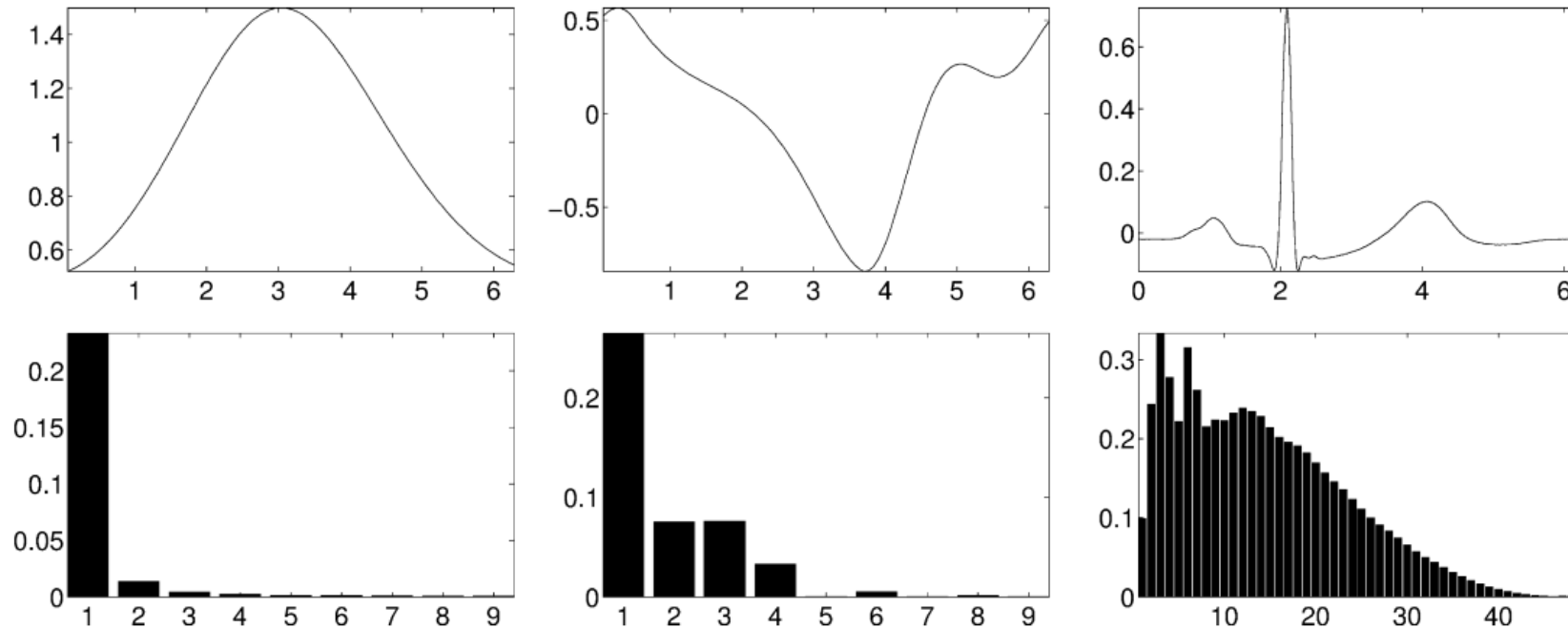
Examples of WSF [3]

Wave-Shape Function (WSF)

Its Fourier series satisfies $s(t) = \sum_{l \in \mathbb{Z}} \hat{s}(l) e^{jl2\pi t}$, where $\hat{s}(l)$ are the Fourier coefficients.

S1: The fundamental component cannot be zero.

S2: Coefficients decay fast enough.



Three different shape functions [3]

Adaptive Non-Harmonic (ANH) Model

Replace cosine by an 1-periodic function (WSF) from the adaptive harmonic model.

The model was generalized to:

$$f(t) = \sum_{k=1}^K f_{fix,k}(t)$$

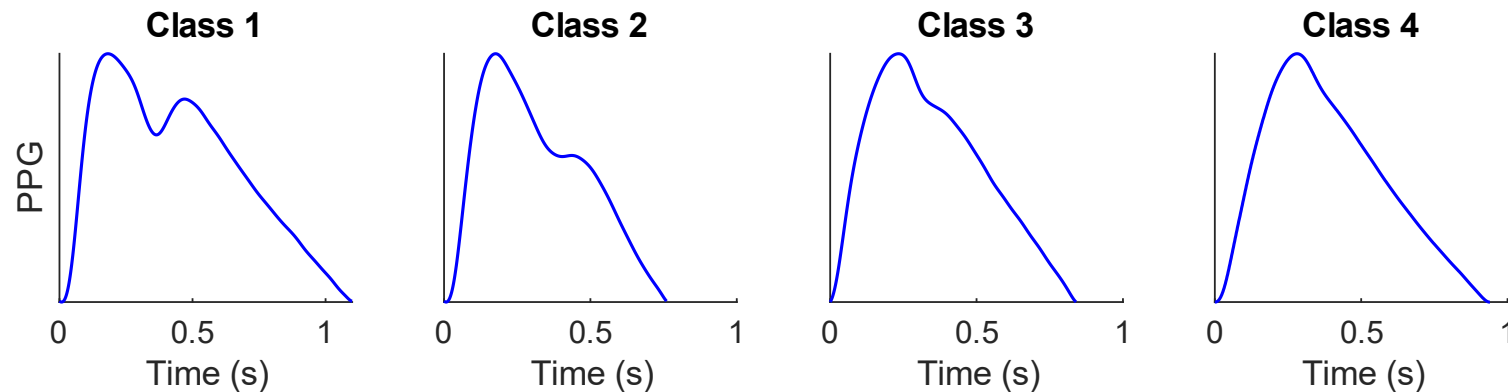
where $f_{fix,k}(t) = A_k(t)s_k(\phi_k(t))$.

Since the WSF $s(t)$ is periodic, we can expand this by the Fourier series:

$$f_{fix,k}(t) = A_k(t) \sum_{l=1}^{\infty} \alpha_{k,l} \cos(2\pi l \phi_k(t) + \beta_{k,l})$$

For real world case

- Electrocardiographic Signal
- Respiratory Signal
- Natural Vibration of Stiff Strings



Examples of the four classes of pulse wave shape proposed by Dawber et al. Reproduced from [4]

Time-Varying Wave-Shape Functions

The model was generalized to:

$$f_{var}(t) = \sum_{l=1}^{\infty} A_l(t) \cos(2\pi\phi_l(t))$$

- The IFs $\phi_l'(t)$ are not far from a multiple of the fundamental frequency $l\phi_1'(t)$.

The Adaptive non-Harmonic Model (ANH_KM) we consider in this paper satisfies

$$f(t) = \sum_{k=1}^K f_{var,k}(t)$$

where $f_{var,k}(t) = \sum_{l=1}^{\infty} A_{k,l}(t) \cos(2\pi\phi_{k,l}(t))$.

- The fundamental IFs ($l = 1$) and their multiple components ($l \neq 1$) need to be separated.

De-shape Algorithm [5]

- For a chosen window function h , the definition of Short time Fourier transform (STFT):

$$V_f^h(t, \xi) = \int f(\tau)h(\tau - t)e^{j2\pi\xi(\tau-t)} d\tau$$

- The short time cepstral transform (STCT):

$$C_f^h(t, q) = \int \ln(|V_f^h(t, \xi)|) e^{j2\pi\xi q} d\xi$$

where q is called the quefrequency.

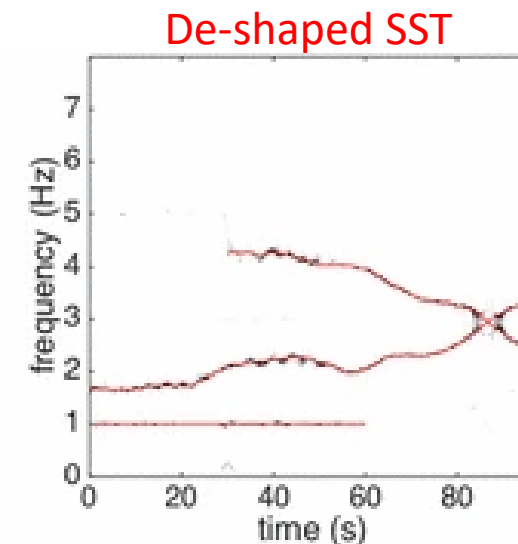
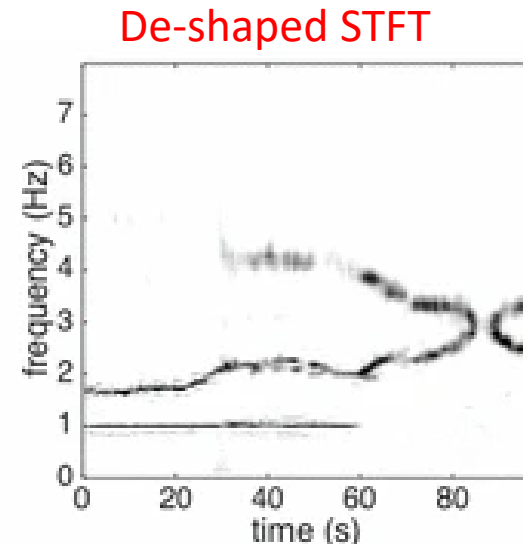
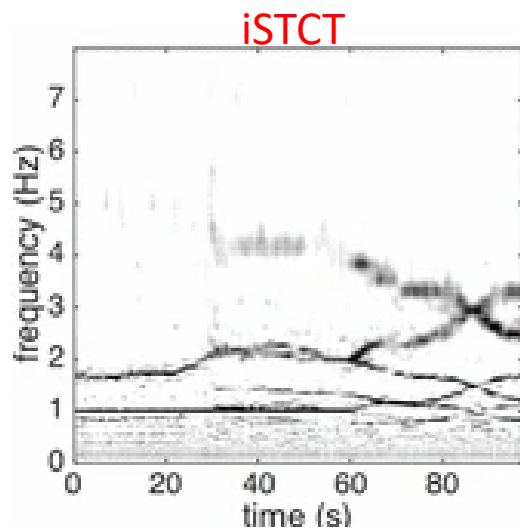
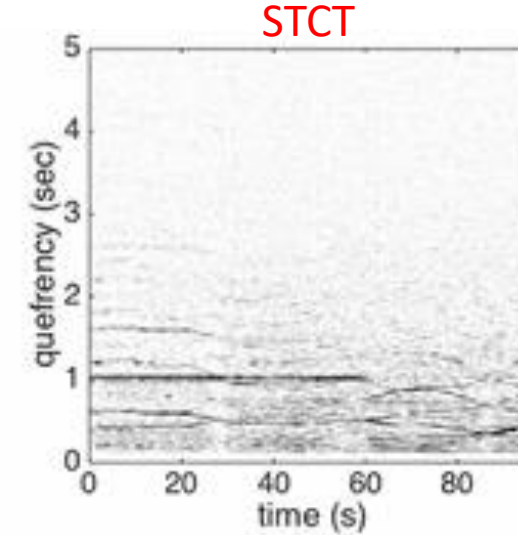
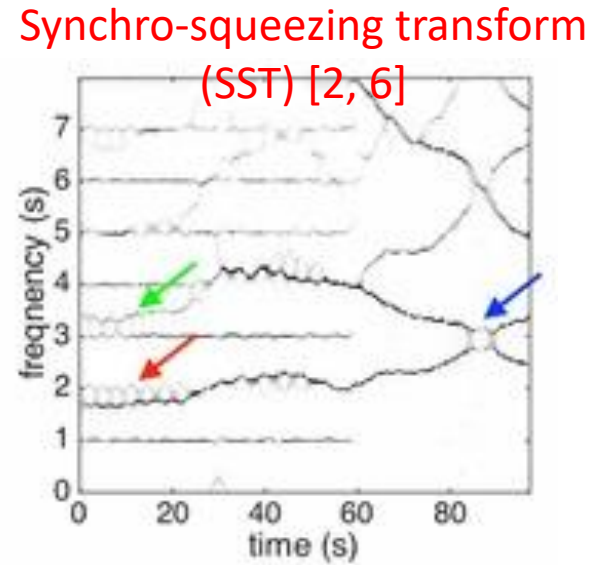
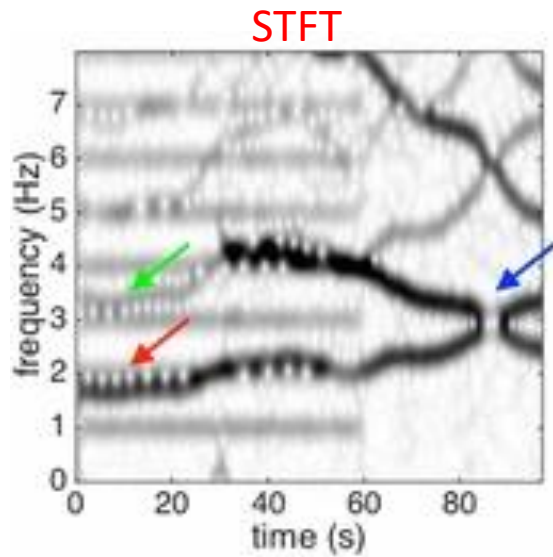
- The inverse short time cepstral transform (iSTCT):

$$U_f^h(t, \xi) = C_f^h\left(t, \frac{1}{\xi}\right)$$

- The de-shape STFT:

$$W_f^h(t, \xi) = V_f^h(t, \xi)U_f^h(t, \xi)$$

Three components simulated signal [5]

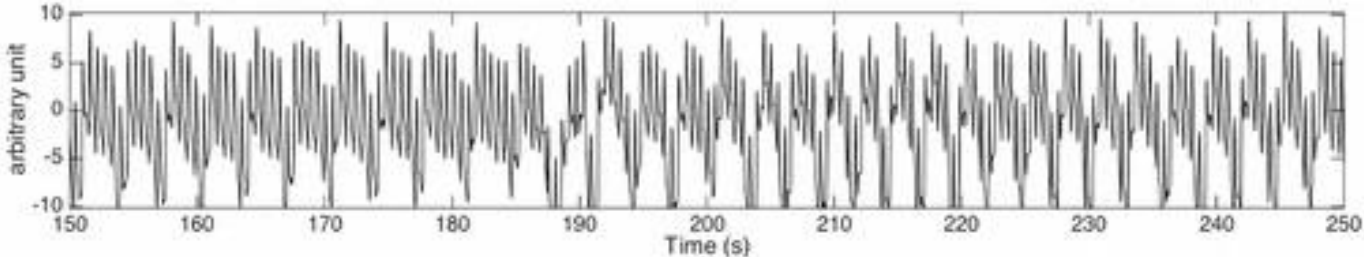


[5] Lin, CY., Su, L. & Wu, HT. Wave-Shape Function Analysis. J Fourier Anal Appl 24, 451–505 (2018).

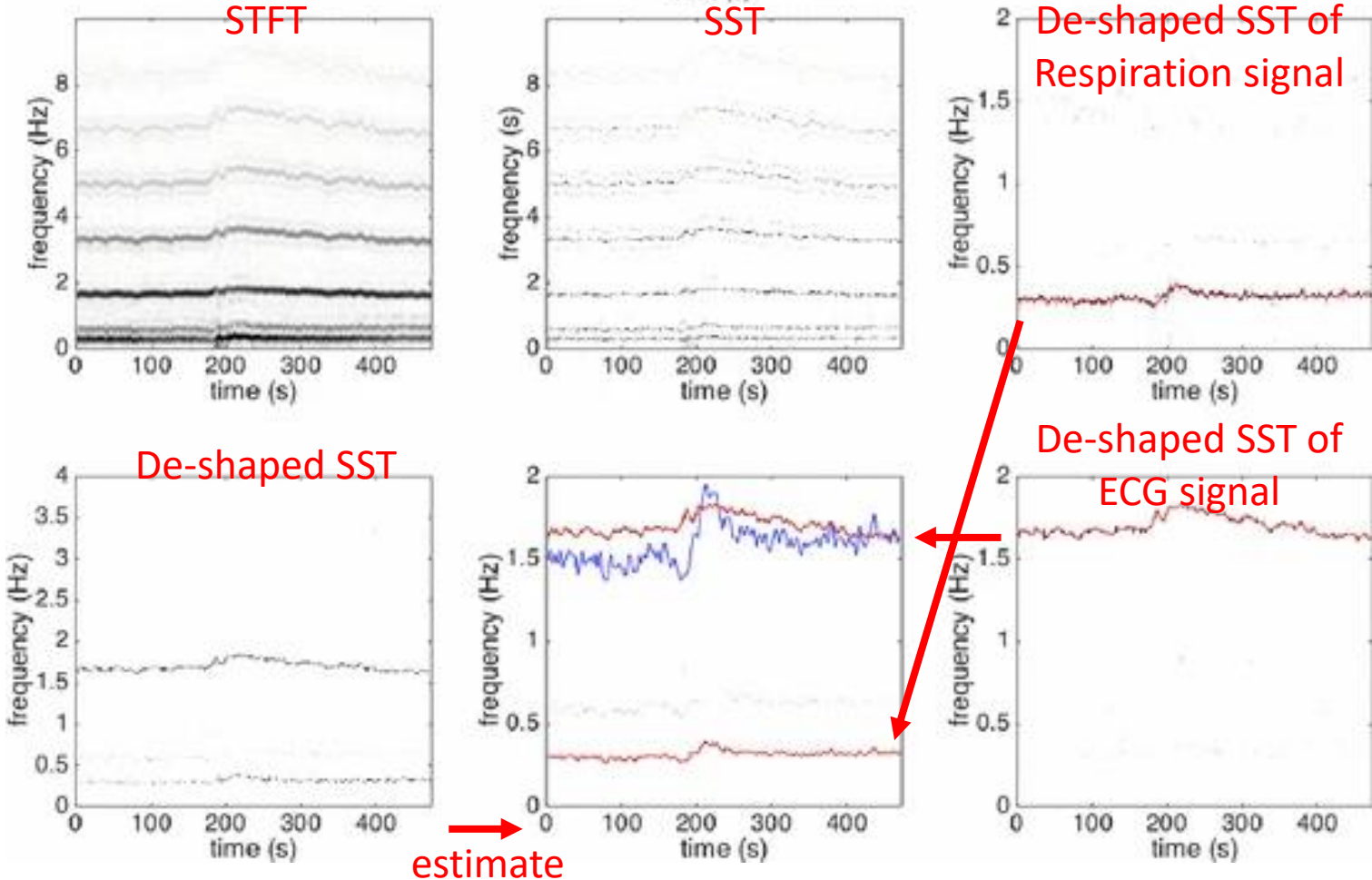
[6] T. Oberlin, S. Meignen and V. Perrier, "The fourier-based synchrosqueezing transform," 2014 IEEE International Conference on Acoustics, Speech and Signal Processing (ICASSP), Florence, Italy, 2014, pp. 315-319

photoplethysmography (PPG) signal

PPG signal



The PPG signal, the capnogram signal (respiration signal) and the ECG signal are simultaneously recorded from a subject without any motion at 300 Hz for 480 s. [5]



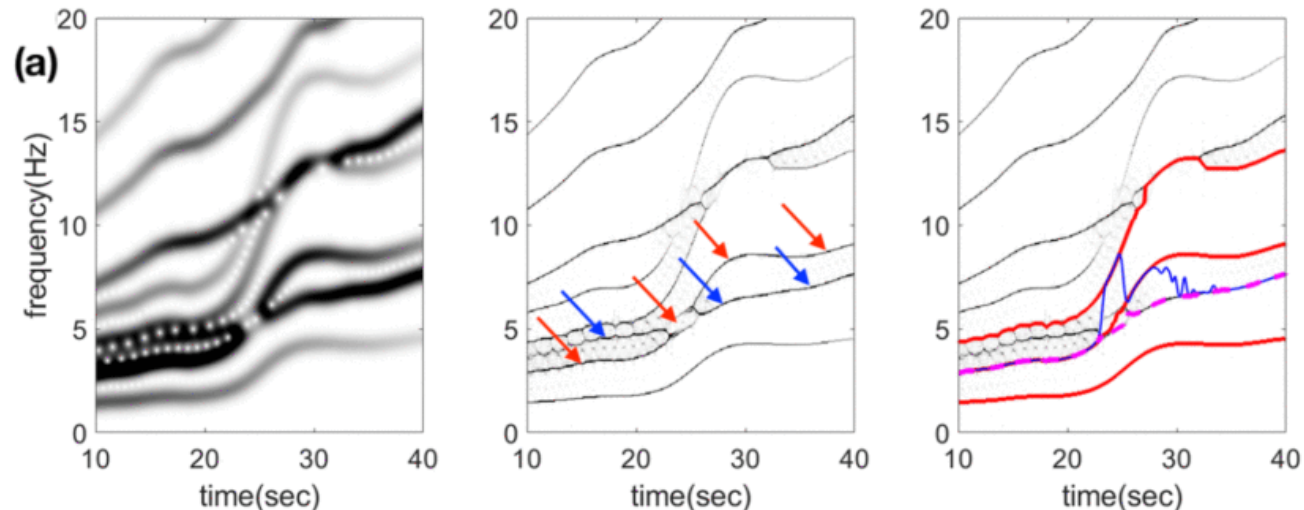
[5] Lin, CY., Su, L. & Wu, HT. Wave-Shape Function Analysis. J Fourier Anal Appl 24, 451–505 (2018).

Ridge extraction (Instantaneous frequency estimation)

For the Time-Frequency representation \mathbf{R} , a frequently used method is to solve the following path optimization problem [7, 8]:

$$c^* = \arg \max_c \left(\sum_{j=1}^N |\tilde{\mathbf{R}}(j, c(j))| - \lambda_1 \sum_{j=1}^{N-1} |c(j+1) - c(j)|^2 \right)$$

where $\tilde{\mathbf{R}}(l, q) = \log \frac{|\mathbf{R}(l, q)|}{\sum_{i,j} |\mathbf{R}(i, j)|}$ is a normalization of the matrix, $\lambda_1 > 0$ is the penalty term constraining the regularity of the fit.



[7] R. A. Carmona, W. L. Hwang and B. Torresani, "Characterization of signals by the ridges of their wavelet transforms," in IEEE Transactions on Signal Processing, vol. 45, no. 10, pp. 2586-2590, Oct. 1997

[8] Y. -W. Su, G. -R. Liu, Y. -C. Sheu and H. -T. Wu, "Ridge Detection for Nonstationary Multicomponent Signals With Time-Varying Wave-Shape Functions and its Applications," in IEEE Transactions on Signal Processing, vol. 72, pp. 4843-4854, 2024

Shape-Adaptive Mode Decomposition (SAMD)

- The optimization problem [1]:

$$\min_{c_{i,l}, d_{i,l}, \Phi_{i,l}} \left\| \left\| y(t) - \sum_{i=1}^I \tilde{A}_i(t) \sum_{l=1}^{D_i} \left(c_{i,l} \cos(\Phi_{i,l}(t)) + d_{i,l} \sin(\Phi_{i,l}(t)) \right) \right\| \right\|_2^2$$

- For more complex phases than those merely being integer multiples. Then, the evidently nonlinear regression problem

$$\min_{c_{i,l}, d_{i,l}, e_{i,l,k}} \left\| \left\| y(t) - \sum_{i=1}^I \tilde{A}_i(t) \sum_{l=1}^{D_i} \left(c_{i,l} \cos \left(\sum_{k=1}^K e_{i,l,k} \tilde{\Phi}_{i,1}^k \right) + d_{i,l} \sin \left(\sum_{k=1}^K e_{i,l,k} \tilde{\Phi}_{i,1}^k \right) \right) \right\| \right\|_2^2$$

- The Amplitude $\tilde{A}_i(t)$ and Phase $\tilde{\Phi}_i(t) \approx 2\pi\tilde{\phi}_{i,1}(t)$ can be estimated by ridge detection with the SST.

$$\Phi_{i,l}(t) \approx \sum_{k=1}^K e_{i,l,k} \tilde{\Phi}_{i,1}^k$$

- Approximate $s_i(t)$ by its first D_i harmonics and solve the linear regression problem:

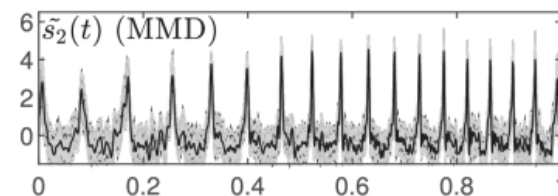
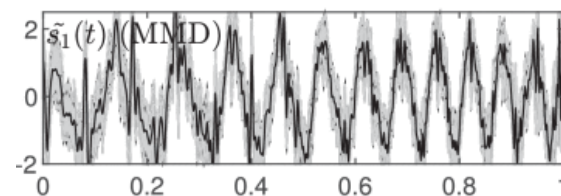
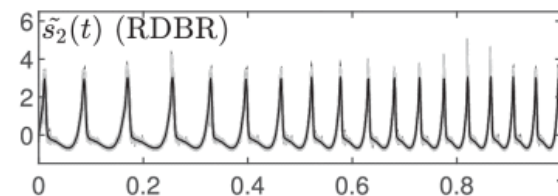
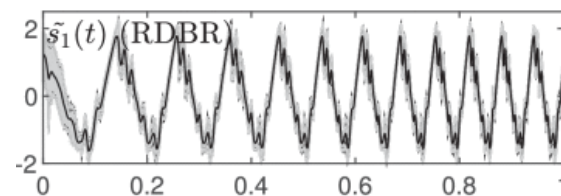
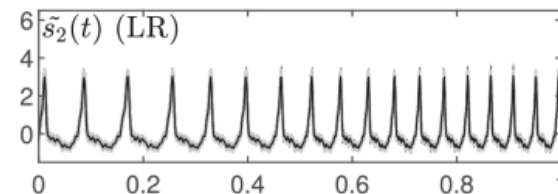
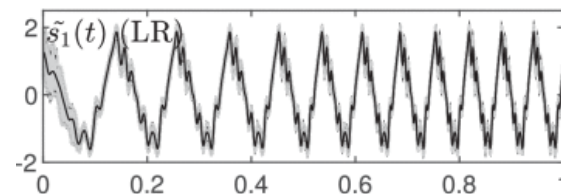
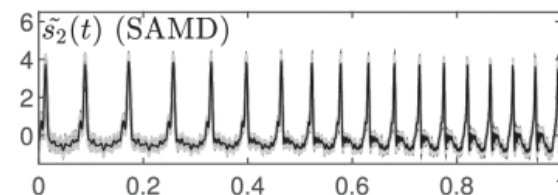
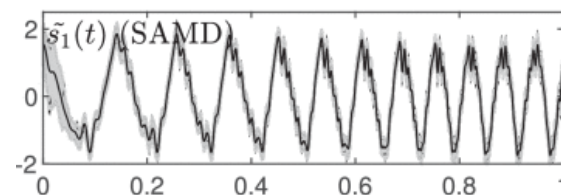
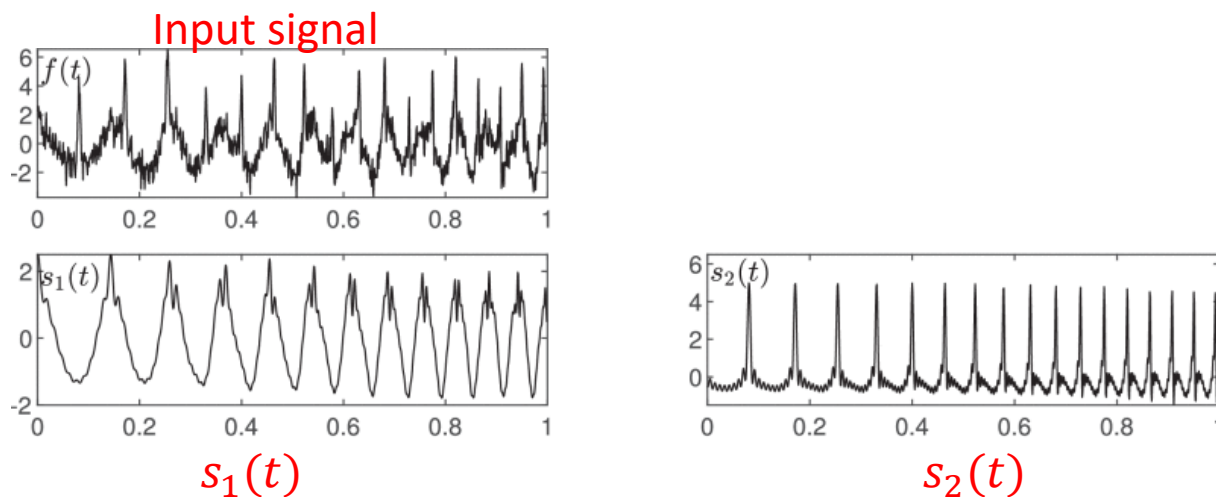
$$\min_{c_{i,l}, d_{i,l}} \left\| \left\| y(t) - \sum_{i=1}^I \tilde{A}_i(t) \sum_{l=1}^{D_i} \left(c_{i,l} \cos(l\tilde{\Phi}_i(t)) + d_{i,l} \sin(l\tilde{\Phi}_i(t)) \right) \right\| \right\|_2^2$$

Algorithm 1: Shape-Adaptive Mode Decomposition (SAMD).

1. Ridge extraction for amplitudes and phases
2. Linear regression step for Fourier series parameters $c_{i,l}, d_{i,l}$
3. Non-linear regression step for parameters of high order polynomial phases $e_{i,l,k}$
4. Synthesize the modes

- 1: **Input:** signal $y(t)$, and K (for phases estimations).
 - 2: Estimate the amplitudes $\tilde{A}_i(t)$ and phases $\tilde{\phi}_{i1}(t)$ from second-order SST, ridge detection, and partial reconstruction (Section III-A), which also give an estimate of I .
 - 3: Solve the linear regression problem to obtain the coefficients $\hat{c}_{i,l}$ and $\hat{d}_{i,l}$, which also give an estimate of parameters D_i (Section III-D1).
 - 4: Solve the nonlinear regression problem from (17) using $\hat{c}_{i,l}$ and $\hat{d}_{i,l}$, and $e_{i\ell 1} = \ell$, $e_{i\ell k} = 0$ for $k = 2, \dots, K$, as initial values.
 - 5: With the coefficients $\tilde{c}_{i,l}$, $\tilde{d}_{i,l}$ and $\tilde{e}_{i\ell k}$ synthesize the modes $f_{\text{var},i}(t)$.
 - 6: **Output:** modes $f_{\text{var},i}(t)$, $i = 1, \dots, I$.
-

Experiments



	Noiseless	Noisy (10 dB; 100 realizations)		
	RMSE	mean(RMSE)	std(RMSE)	mean time (s)
s_1 (SAMD)	0.206	0.288	0.017	43.210
s_2 (SAMD)	0.501	0.542	0.039	
s_1 (LR)	0.328	0.349	0.019	0.003
s_2 (LR)	0.627	0.638	0.043	
s_1 (RDBR)	0.330	0.355	0.021	14.245
s_2 (RDBR)	0.631	0.638	0.042	
s_1 (MMD*)	0.483	0.646	0.473	462.786
s_2 (MMD*)	0.483	0.611	0.063	

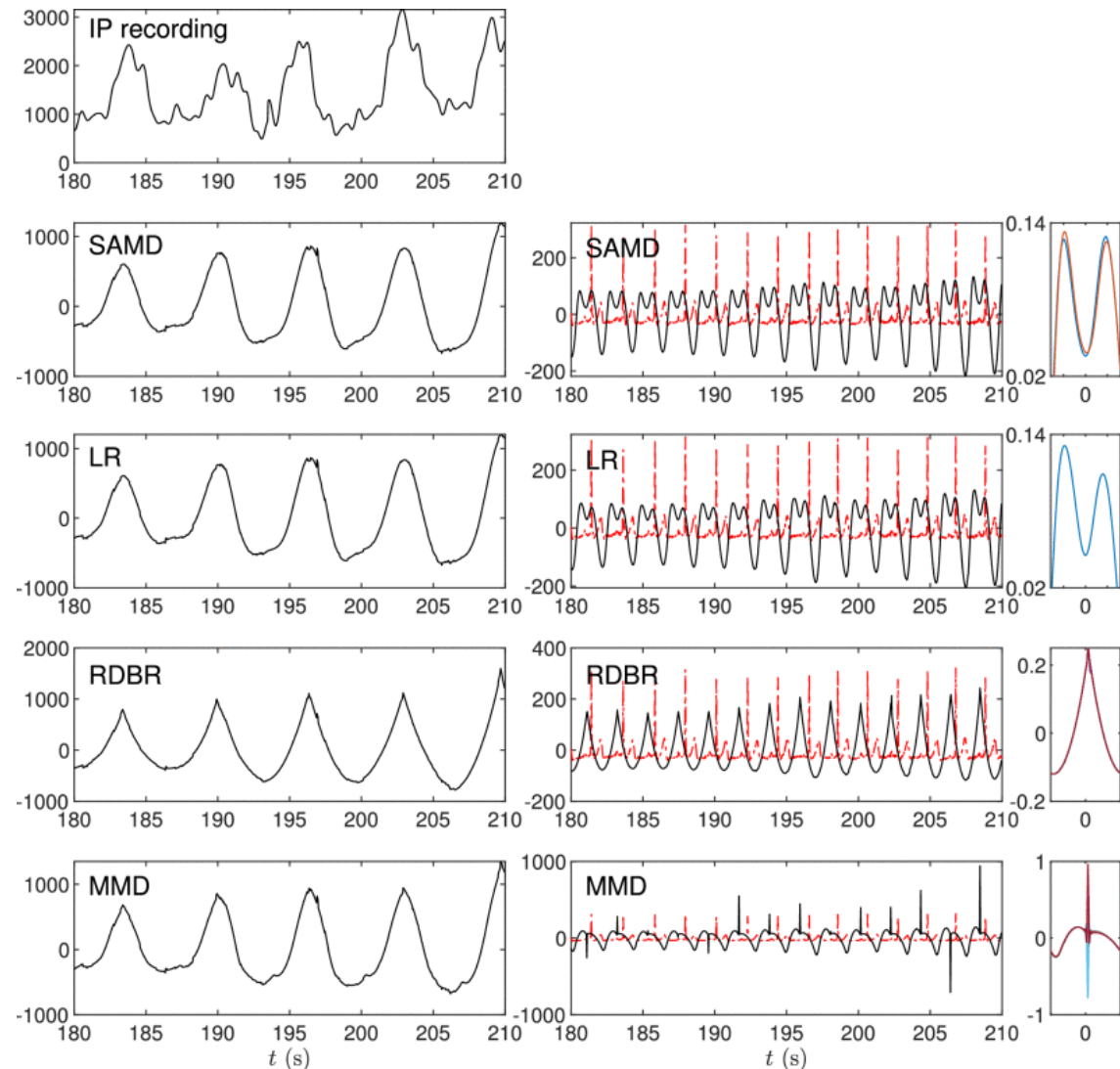
$s_1(t)$

$s_2(t)$

Experiments (impedance pneumography (IP))

An IP signal is usually composed of one respiratory component and one cardiac component, called the cardiogenic artifact.

For the 60-second segment, the computational times were 3.62 s, 0.007 s, 179.1 s, and 34.14 s for SAMD, LR, RDBR and MMD respectively.



Conclusion

- To handle oscillatory signals in the real world, a model is provided capturing oscillatory features, including IF, AM and time-varying wave-shape function.
- The idea of cepstrum introduce the STCT, de-shape STFT and de-shape SST.
- A novel nonlinear regression algorithm was proposed, SAMD, to decompose signals with time-varying WSFs.

References

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